

1 **Microalgae Separation by Inertia-enhanced Pinched Flow**

2 **Fractionation**

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18 **Keywords: iPFF; microalgae; microfluidic chip; separation**

19 **Abbreviations: iPFF**

20 Abstract

21 To improve the accuracy and efficiency of ships' ballast water detection, the separation
22 of microalgae according to size is significant. In this paper, a method to separate microalgae
23 based on inertia-enhanced pinched flow fractionation (iPFF) was reported. The method
24 utilized the inertial lift force induced by flow to separate microalgae according to size
25 continuously. The experimental results show that, as the Reynolds number increases, the
26 separation effect becomes better at first, but then stays unchanged. The best separation effect
27 can be obtained when the Reynolds number is 12.3. In addition, with the increase of the flow
28 rate ratio between sheath fluid and microalgae mixture, the separation effect becomes better
29 and the best separation effect can be obtained when the flow rate ratio reaches 10. In this case,
30 the recovery rate of *Tetraselmis* sp. is about 90%, and the purity is about 86%; the recovery
31 rate of *Chlorella* sp. is as high as 99%, and the purity is about 99%. After that, the separation
32 effect keeps getting better but very slowly. In general, this study provides a simple method
33 for the separation of microalgae with different size, and lays a foundation for the accurate
34 detection of microalgae in the ballast water.

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43 **1 Introduction**

44 The discharge of the microalgae in the ships' ballast water from one port to the others
45 during the international trade, is one of the main causes of biological invasion [1]. It is
46 necessary to detect microalgae before the discharge of the ship's ballast water into the sea [2].
47 However, there are many kinds of microalgae in the ballast water and they have a wide range
48 of sizes. So it is a great challenge to detect these microalgae directly as every detection
49 method has a certain size detection interval. In order to solve that, the separation of
50 microalgae according to size before detecting is necessary.

51 In the last decades, the research on the microalgae separation is popular and many
52 methods have been proposed and developed. Based on whether an external physical field is
53 needed, these methods fall into two categories: active separation and passive separation [3].
54 The former one often requires external physical fields, such as electric field, magnetic field,
55 and sound field [4-6]. The technique based on electrophoresis or dielectrophoresis can
56 separate microalgae cells according to their different volumes or dielectric constants.
57 Recently, Jiang et al. developed a recycling free-flow isoelectric focusing method based on
58 electrophoresis to achieve the enrichment of low-abundant bacteria [7]. This method
59 successfully increased the bacterial abundance by 225%. Dong et al. developed a free-flow
60 electrophoresis (FFE) technique and separated *Escherichia coli* and *Staphylococcus aureus*
61 effectively. This work provided a new idea for cell separation [8]. Similarly, He et al.
62 separated complete mitochondria from mitochondria resuspension buffer using the method of
63 free-flow isoelectric focusing. This method has advantages in measuring the isoelectric point
64 of substances such as proteins [9]. Xuan et al. have used the technique based on magnetic
65 field to successfully separate polystyrene particles of 3 and 10 μm [10]. In addition, immuno-
66 magnetic beads are usually used for the separation of tumor cells or exosomes [11]. It can
67 separate high purity target cells and other substances from complex mixtures. The sound field

68 separation method is mainly based on high frequency sound waves. Dow et al. isolated and
69 purified bacteria from the blood using acoustic method, which greatly increased the detection
70 limit of *Escherichia coli* [12]. However, the external force fields required in the active
71 separation may bring harm to the activity of bio-particles, which limits the development of
72 this method in the field of microalgae separation [4]. So the researchers turn to the passive
73 separation which does not require an external physical field. Centrifugation is the most
74 common separation method. However, it is difficult to be integrated with microfluidic chips
75 [13]. There are also some methods typically exploit special flow channel structures to
76 separate microalgae based on their size. The separation technologies of inertial microfluidics
77 based on channel innovations have been recognized as a powerful tool for high throughput
78 microalgae separation. The separation of *Chlorella* sp. and *Cosmarium* sp. using dean flow in
79 a spiral microfluidic device was reported by Lee et al. [14]. This technique has a high flux
80 and simple structure because it only needs pressure-driven. Nevertheless, the technique can
81 only separate the diluted sample due to the interaction between among cells. Recently, Li et
82 al. reported a sinusoidal-shaped inertial microfluidic device to purify cancer cells [15].
83 Warkiani ME et al. proposed a spiral-shaped inertial microfluidic channel to separate tumor
84 cells from urine [16].

85 Specially, a method named pinched flow fractionation (PFF) utilizing the laminar flow
86 profile in microchannel to separate particles by size continuously was proposed by Yamada et
87 al. [17]. On a PFF microfluidics, particles with different size must be focused to one sidewall
88 of channel by using a pressure-driven sheath flow. The particles, as a result, locate at the
89 different streamlines that are dominated by the size. Further, the distance between particles
90 with different size is enlarged at the downstream abruptly broadened part. However, PFF can
91 only work normally at a larger flow rate ratio, and the separation distance in the abruptly
92 broadened part is very limited [18]. Recently, Inertia-Enhanced Pinched Flow Fractionation

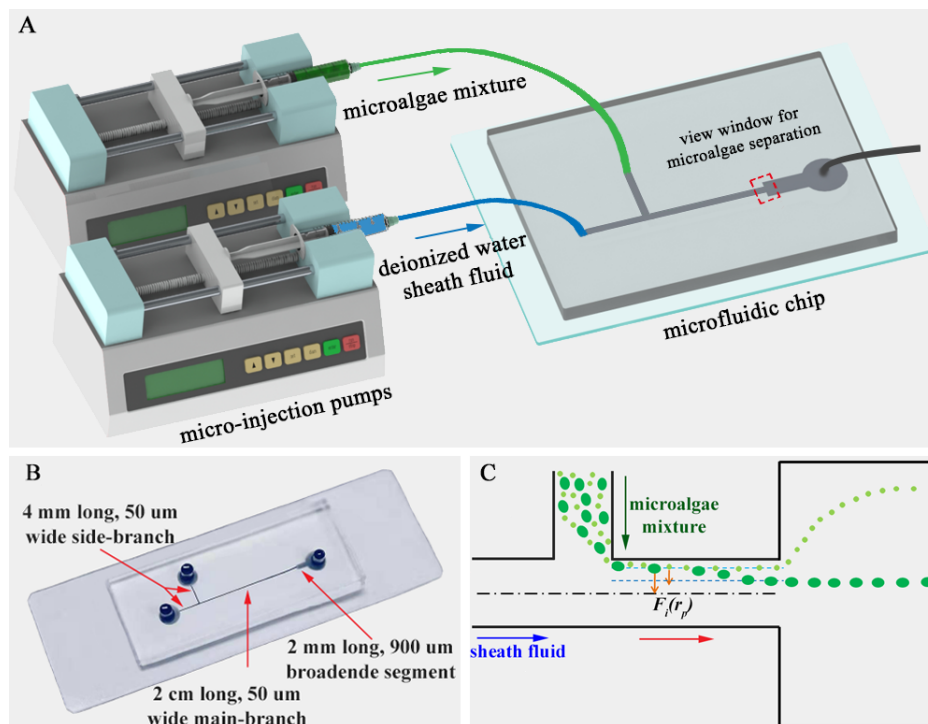
93 technique (iPFF) based on PFF was firstly proposed by Xuan et al. to improve the separation
94 effect of PFF [18, 19]. The method exploits the inertial lift force, an additional force induced
95 by flow, to enhance the polystyrene particles offset in PFF and consequently increases the
96 separation effect. Compared with PFF, iPFF can work normally at a lower flow rate ratio, so
97 a higher particle flux can be obtained, which can be increased by at least 10 times. Besides,
98 the separation distance in the abruptly broadened part is also significantly improved [18].
99 Compared with the existing inertial microfluidics technology, iPFF has the advantages of
100 high separation efficiency and high operational throughput. What is more valuable is that this
101 method hardly causes any damage to the cells. However, the application of iPFF in
102 microalgae cells separation has not been studied systematically.

103 The purpose of this paper is to demonstrate the potential application of iPFF technique
104 for microalgae separation in ballast water. In addition, the effects of fluid inertia (Re) and
105 flow rate ratio (α) on the separation effect are explored systematically, and the optimal
106 separation parameters are obtained for the separation of *Chlorella* sp. and *Tetraselmis* sp.

107 **2 Materials and Methods**

108 **2.1 Separation system**

109 The microalgae separation system, shown in Figure 1A, consists of a microfluidic chip,
110 a microscopy (not drawn in the figure 1A), two micro-injection pumps, two syringes, and
111 some rigid Teflon capillaries for connecting the syringes and microfluidic chip.



112

113 **Figure 1.** The diagram of the microalgae separation system (A) and the microfluidic chip (B)

114 designed for the experiment. The chip is filled with black ink for clarity. The schematic diagram

115 of the microalgae separation via iPPF is drawn not scale (C). The inertial lift forces are indicated

116 by F_i . The solid arrows indicate the flow direction in the sheath flow (blue), microalgae mixture

117 (green) and main channel (red).

118 As shown in Figure 1B, the microfluidic chip was designed with two inlet wells, one

119 outlet well, two side branch channels and one main channel. The length and width of the side

120 branch channels are 4 mm and 50 μm , respectively, and that of the main channel are 20 mm

121 and 50 μm , respectively. At the end of the main channel, there is an abruptly broadened

122 segment with 2 mm in length and 900 μm in width. The overall height of the microchannel is

123 20 μm . It should be noted that the abruptly broadened segment is designed for further

124 separating cells and it also serves as the observing window. A microscopy (Nikon Eclipse

125 TE2000U, Nikon Instruments) is located just above the observing window monitoring the

126 separation effect. Driven by the pumps (Harvard Apparatus, Pump 11 Pico Plus), the syringes

127 (Ordinary medical syringe with a specification of 1 mL) deliver the sample to the
128 microfluidic chip.

129 **2.2 Chip fabrication and sample preparation**

130 The mold for microchannel was fabricated on a silicon substrate (4"N/PHOS, Montco
131 Silicon Technology Inc., Spring City, PA, USA) using a mask-less laser writing machine
132 (MLA150, Heidelberg instruments, Germany) [20, 21]. Afterwards, the polydimethylsiloxane
133 (PDMS, Sylgard 184, Dow Corning, USA) was mixed with the curing agent in a weight ratio
134 of 10: 1 and degassed [21]. Then, the mixture was poured on the silicon mold and baked in an
135 oven (Isotemp model 280A, Fisher Scientific, Pittsburgh, PA, USA) at 70 °C for 4 hours to
136 keep full curing [22]. After that, the PDMS was peeled off and perforated separately in the
137 inlet and outlet wells with a hole punch. Finally, the PDMS together with a clean glass slide
138 (25.66 × 75.47 × 1.07 mm, CITOGLAS, China) was put into a plasma cleaner (HARRICK
139 PLASMA, Ithaca, NY, USA) and processed for 100s. The irreversible combination of the
140 two would produce a microfluidic chip.

141 The *Chlorella* sp. and *Tetraselmis* sp. used in the experiment were bought from
142 Shanghai Guangyu Biological Technology Co., Ltd. The shape and size of the microalgae
143 were examined by an optical microscopy. As the microalgae were in different growth stages,
144 their sizes were distributed in a range. Specially, *Chlorella* sp. are spherical, whose
145 equivalent diameter varies from 3 μm to 5 μm. *Tetraselmis* sp. are flat, of which, the average
146 length and width, are approximately 11-14 μm and 7-9 μm, respectively. To remove
147 impurities from the microalginogen solution, the samples were washed by a centrifuge with
148 the speed of 5000 r/min for more than three times. After washing, mix two microalgae
149 solution and keep shaking for one minute to obtain a uniform mixed solution of *Chlorella* sp.

150 and *Tetraselmis* sp.. The final concentration of the microalgae used in this study is about 6.0
151 $\times 10^4$ cells/mL.

152 **2.3 Experimental method**

153 The microalgae mixture solution and deionized water were firstly sucked into two
154 syringes, respectively. Then, the syringes were fixed on the micro-injection pumps and
155 connected to the inlet wells on the microfluidic chip by Teflon capillaries. After that, the
156 pumps were turned on to drive the sample (both the microalgae mixture solution and
157 deionized water) into the side branch channels in the microfluidic chip. To avoid the
158 microalgae entering the sheath fluid channel, the deionized water was driven before the
159 microalgae mixture. The outlet well on the chip was connected to a waste bottle by capillaries.
160 The separated results of *Chlorella* sp. and *Tetraselmis* sp. could be viewed at the abruptly
161 broadened segment using an inverted microscope (Nikon Eclipse TE2000U, Nikon
162 Instruments) with a CCD camera (Nikon DS-Qi1Mc). It should be noted that the separation
163 effect was recorded only when the system was stable. When studying the effects of the fluid
164 inertia and the flow rate ratio, the pumps were adjusted directly to the desired value without
165 changing syringes and microfluidic chip. The streak images were obtained by superimposing
166 a sequence of about 4500 images with the Matlab2016a software [18]. The percentage
167 distribution of microalgae cells was calculated by the software ImageJ which was used to
168 divide the abruptly broadened segment of the series of images into 20 parts longitudinally and
169 count the number of cells in each part separately. The diagrams were processed by the Origin
170 Pro 2020.

171 3 Results and Discussion

172 3.1 Theoretical analysis

173 The mechanism of iPPF is schematically shown in Figure 1C. The microalgae mixture
 174 is firstly focused to one sidewall using a sheath fluid flow at the T-shaped channel. Then, the
 175 inertial lift force induced by flow [23-26], F_i , pushes the microalgae toward the center of the
 176 channel. It should be noted that, F_i can be calculated as following:

$$177 \quad F_i = C_L \rho r_p^4 \gamma^2 \quad (1)$$

178 Where C_L is a dimensionless lift coefficient which is a dominated by the Re and the position
 179 of the microalgae, ρ is the density of the sample fluid, r_p is the equivalent radius of the
 180 microalgae, and γ is the shear rate. Obviously, F_i is a strong depend on the cell size and the
 181 lateral offset between microalgae with different size can be increased in a larger interval. In
 182 addition, the separation distance between microalgae was further enlarged in the abruptly
 183 broadened segment [18].

184 There are two defined dimensionless numbers in this iPPF technique that can affect the
 185 separation effect significantly [27-30]. The first one is the Reynolds number, Re , defined as
 186 the ratio of the inertial force to the viscous force, as it dominates the inertial migration of the
 187 cells in confined channel flows [31, 32]. The Re could be as following,

$$188 \quad Re = \frac{\rho U_f D_h}{\mu} = \frac{2\rho Q}{\mu(w+h)} \quad (1)$$

189 Where U_f is the average velocity of the fluid in the main channel, D_h is the hydraulic
 190 diameter, for the rectangular cross-section flow channel D_h can be estimated as

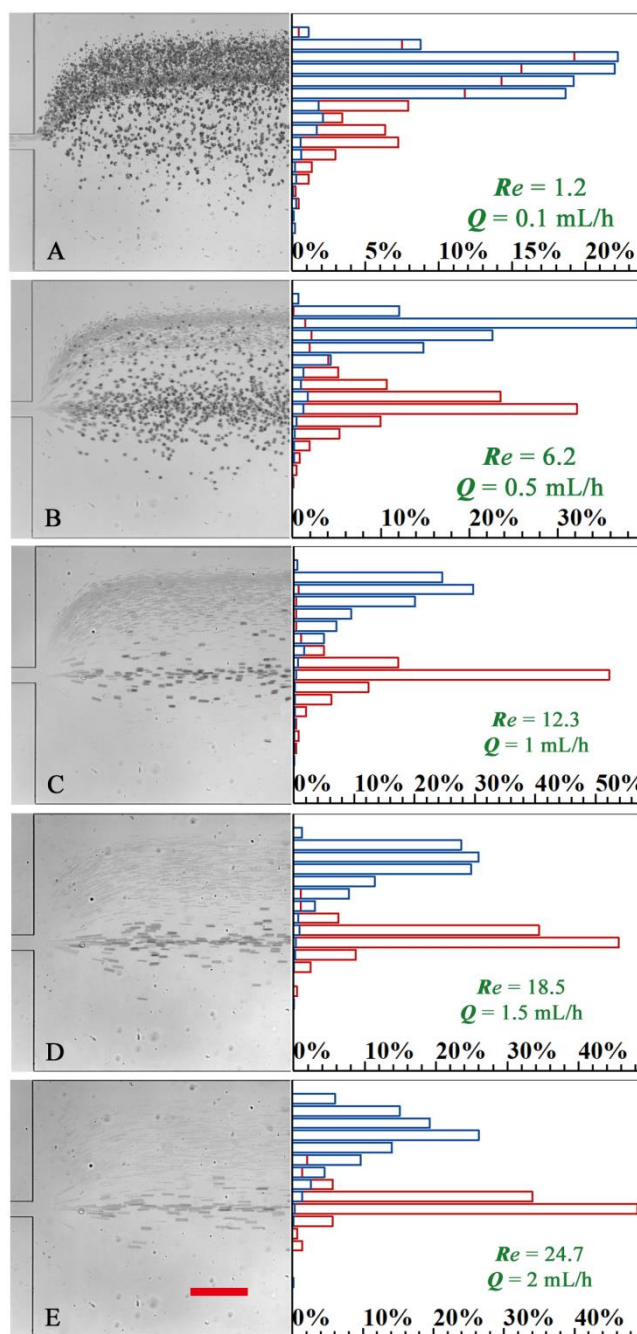
191 $D_h = 2wh / (w+h)$ with h and w indicating the height and width of the rectangular channel,

192 and Q is the flow rate in volume. The second important dimensionless number is the flow

193 rate ratio (α), which characterizes the ratio of the volumetric flow of the sheath fluid,
194 Q_{sheath} , to that of the microalgae mixture $Q_{microalgae}$, in the two side branch channels. It
195 indicates the strength of the focusing effect and affects the cell dispersion in the abruptly
196 broadened segment. Obviously, $Q = Q_{sheath} + Q_{microalgae}$.

197 **3.2 The Effect of Fluid Inertia (Re)**

198 As mentioned in Section 2, the Reynolds number has a large impact on the separation.
199 The effects of the Reynolds number were studied by changing the total flow rate in the main
200 channel when the flow rate ratio between the sheath fluid and the microalgae mixture was
201 fixed to 10 approximately. The experimental results are shown in Figure 2. The left part of
202 each picture is the cell streak image obtained at the abruptly broadened segment, and the light
203 color part is *Chlorella* sp., the deep color part is *Tetraselmis* sp. The right part of each picture
204 shows the percentage distribution of microalgae cells in different locations, and the blue bars
205 represent the percentage distribution of *Chlorella* sp., the red bars represent that of
206 *Tetraselmis* sp. It demonstrates that the *Chlorella* sp. can be separated from the *Tetraselmis*
207 sp. when the Reynolds number increase to 12.3 (Figure 2C). However, the separation effect
208 seems not to raise with further increasing the Reynolds number.



209

210 **Figure 2.** The effects of the fluid inertia (Re) on the separation of the *Chlorella* sp. and the211 *Tetraselmis* sp. via iPPF while Re increase from 1.2 (A) to 6.2 (B), 12.3 (C), 18.5 (D), and 24.7

212 (E). The left part of each figure is the images at the abruptly broadened segment. The light color

213 part is *Chlorella* sp., the deep color part is *Tetraselmis* sp. The right part of each figure is

214 percentage distribution of microalgae cells in different locations. The blue bars represent the

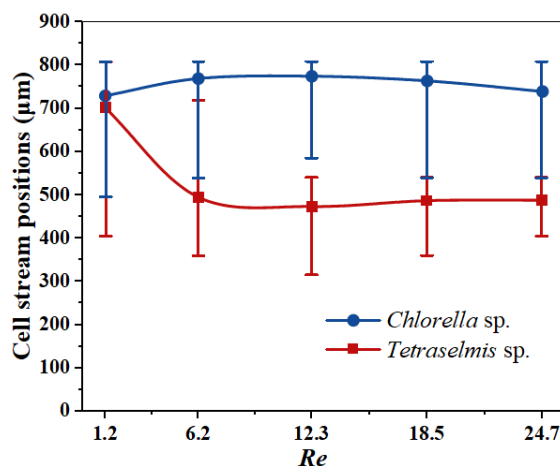
215 percentage distribution of *Chlorella* sp. and the red bars represent that of *Tetraselmis* sp. The

216 flow rate ratio between sheath fluid and microalgae mixture is maintained at 10 approximately.

217 Cells flow from left to right in all images. The scale bar represents 200 μm .

218 To further analyze the separation effects, using the cell deflection from the bottom wall
219 to determine the cell stream position [31], and a quantitative analysis of the two cell streams
220 at the abruptly broadened segment was performed, as shown in Figure 3. The effect of the
221 Re on the separation could be concluded as following. When the Reynolds number is less
222 than 12.3 (the total flow rate is less than 1 mL/h), the widths of the cell streams decrease
223 regularly with the increase of the Reynolds number. When the Reynolds number increases to
224 12.3, which means the widths of the cell streams reach the minimum, the *Chlorella* sp. and
225 the *Tetraselmis* sp. can be completely separated at this condition. After that, as the Reynolds
226 number further increases, the width of the cell stream of *Chlorella* sp. begins increasing, but
227 that of *Tetraselmis* sp. continues to decrease. As a result, the separation effect basically
228 remains unchanged. In summary, as the Reynolds number in the microchannel increases, the
229 separation effect becomes better at first, and then remains largely unchanged.

230 When the Reynolds number increases from 1.2 to 12.3 (the total flow rate reaches 1
231 mL/h), the flow-induced inertial lift force is enhanced so much that it will push the
232 *Tetraselmis* sp. toward the main channel centerline. Meanwhile, the lift force acting on the
233 *Chlorella* sp. is still low due to their much smaller size and it cannot push the *Chlorella* sp.
234 toward the central flow line. Therefore, the *Chlorella* sp. and the *Tetraselmis* sp. can be
235 completely separated in this condition. However, when the Reynolds number further increase
236 over 12.3, the flow-induced inertial lift force acting on the *Chlorella* sp. is also enhanced and
237 the *Chlorella* sp. will toward to the central line. Hence, the separation distance between the
238 *Chlorella* sp. and the *Tetraselmis* sp. decreases and the separation effect is not desirable.

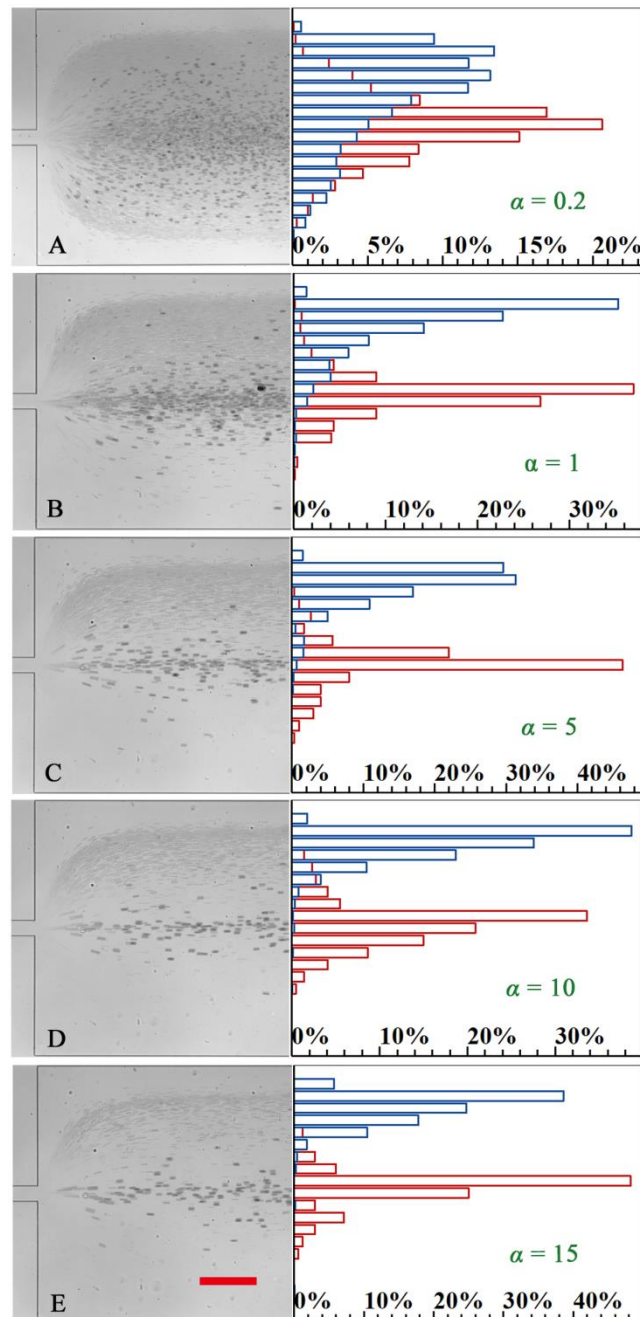


239

240 **Figure 3.** The effects of the fluid inertia (Re) on the stream positions for the *Chlorella* sp. (blue
 241 circle) and *Tetraselmis* sp. (red square). The bottom sidewall of the channel expansion was used
 242 as the reference point (0 μm). Error bars were included for both cells in Figure 2 to cover the
 243 span of each cell stream. Confidence interval of the graph is 95%.

244 3.3 The Effect of Flow Rate Ratio (α)

245 The influence of the flow rate ratio (α) on the separation effect is as important as Re .
 246 The effects of the flow rate ratio were also studied by changing the ratio between the sheath
 247 fluid flow and the microalgae mixture flow when the Reynolds number was fixed to 12.3
 248 approximately. The experimental results are shown in Figure 4. Similar to Figure 2, the left
 249 part of each picture is the cell streak image obtained at the abruptly broadened segment and
 250 the right part shows the percentage distribution of microalgae cells in different locations. It is
 251 obvious that *Chlorella* sp. can be separated from the *Tetraselmis* sp. when the flow rate ratio
 252 increases to 10 (Figure 4D). In this case, the recovery rate of *Tetraselmis* sp. is about 90%,
 253 and the purity is about 86%; the recovery rate of *Chlorella* sp. is as high as 99%, and the
 254 purity is about 99%.



255

256 **Figure 4.** The effects of the flow rate ratio (α) on the separation of *Chlorella* sp. and257 *Tetraselmis* sp. via iPFF while α increase from 0.2 (A) to 1 (B), 5 (C), 10 (D), and 15 (E). The

258 left part of each figure is superimposed images at the abruptly broaden segment. The light color

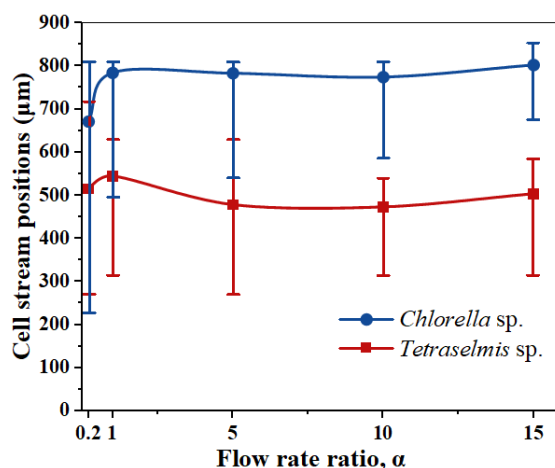
259 part is *Chlorella* sp., the deep color part is *Tetraselmis* sp. The right part of each figure is

260 percentage distribution of microalgae cells in different locations. The blue bars represent the

261 percentage distribution of *Chlorella* sp. and the red bars represent that of *Tetraselmis* sp. The262 Reynolds number (Re) in the main channel is maintained at 12.3 approximately. Cells flow263 from left to right in all images. The scale bar represents 200 μm .

264 A quantitative analysis of the exiting positions of the two cell streams at the abruptly
265 broaden segment is also shown in Figure 5. When the flow rate ratio (α) is below 1, the
266 *Chlorella* sp. and the *Tetraselmis* sp. are almost completely mixed together. When α
267 approaches 5, the main parts of the two cell streams can be separated, but under this condition,
268 as shown in Figure 4C, the cell streams still have some overlap. When α approaches 10 or
269 larger, the cell streams can be separated completely and the separation distance increase
270 slowly as α does. In addition, compared with PFF, iPFF only needs to work at a smaller flow
271 rate ratio ratio, which can increase cell flux significantly [31].

272 Theoretically, the cells (both *Tetraselmis* sp. and *Chlorella* sp.) cannot be focused to a
273 thin layer close to one sidewall of the T-shaped channel when the flow rate ratio is small,
274 such as 0.2, 1 or 5. So distribution ranges of *Tetraselmis* sp. and *Chlorella* sp. are very wide,
275 especially in the abruptly broadened segment. As a result, the separation effect is undesirable.
276 When α approaches 10 or larger, most cells are focused to the sidewall. Then the flow-
277 induced inertial lift force pushes the cells towards to the central of the microchannel. The
278 *Tetraselmis* sp. can be moved to the central line due to their large size while the *Chlorella* sp.
279 still flows near the sidewall. Consequently, the two cells can be completely separated at this
280 condition. Because of the large size deviation of the two types of cells (cells are in different
281 life cycle stages) used in the experiment, though complete separation can be achieved, the
282 cell separation does not show a most visible enhancement when the flow rate ratio is
283 increased from 5 to 15.



284

285 **Figure 5.** The effects of the flow rate ratio (α) on the stream positions for the *Chlorella* sp.
286 (blue circle) and *Tetraselmis* sp. (red square). The bottom sidewall of the channel expansion was
287 used as the reference point (0 μm).

288 4 Conclusions

289 It is a great challenge to detect the microalgae in the ballast water directly. So the
290 separation of the microalgae according to size is necessary before detecting. Unfortunately,
291 the methods for microalgae separation are not developed smoothly. In this study, a method to
292 separate microalgae by inertia-enhanced pinched flow fractionation (iPFF) was proposed.
293 Two types of microalgae, *Chlorella* sp. and *Tetraselmis* sp., were used in the experiment to
294 study the performance of the method. The experimental results show that the separation effect
295 becomes better at first but then remains unchanged when the Reynolds number in the
296 microchannel increases. In addition, the separation effect becomes better with increasing the
297 flow rate ratio between sheath fluid and microalgae mixture. In general, this study provides a
298 simple method to separate the microalgae with different size. Besides a simple microfluidic
299 chip, the method need only two syringe pumps which are easy to achieve in the laboratory or
300 work shop. Next, several sets of electrodes would be fabricated on the bottom of the
301 microfluidic channel where the microalgae are just separated by iPFF. In addition,

302 viscoelastic fluids will be used in further experiments. Because cell separation via iPFF can
303 be enhanced if viscoelastic fluids are employed, which may resolve the issue for cells with
304 large size deviations [33, 34]. So the separated microalgae could be detected accurately and
305 continuously which is useful for the port state officers to manage the ships' ballast water in
306 the future. In brief, this work lays a foundation for the management of the ballast water.

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312 **Conflict of interest**

313 The authors have declared no conflict of interest.

314 **Data Availability Statement**

315 The data that support the findings of this study are available from the corresponding author
316 upon reasonable request.

317 **5 References**

- 318 [1] David, M., Perkovič, M. *Mar. Pollut. Bull.* 2004, 49, 313–318.
- 319 [2] Doblin, M. A., Dobbs, F. C. *Mar. Pollut. Bull.* 2006, 52, 259–263.
- 320 [3] Zhang, T., Hong, Z.-Y., Tang, S.-Y., Li, W., Inglis, D. W., Hosokawa, Y., Yalikun, Y.,
321 Li, M. *Lab. Chip* 2020, 20, 35–53.

- 322 [4] Zeng, J., Deng, Y., Vedantam, P., Tzeng, T.-R., Xuan, X. *J. Magn. Mater.* 2013,
323 346, 118–123.
- 324 [6] Wang, Y., Wang, J., Wu, X., Jiang, Z., Wang, W. *ELECTROPHORESIS* 2019, 40, 969–
325 978.
- 326 [7] Jiang, X., Liu, S., Zhang, Y., Ji, Y., Sohail, A., Cao, C., Wang, P., Xiao, H. *Anal. Chem.*
327 2020, 92, 12017–12025.
- 328 [8] He, Y.-C., Kong, F.-Z., Fan, L.-Y., Wu, J. Y., Liu, X.-P., Li, J., Sun, Y., Zhang, Q.,
329 Yang, Y., Wu, X.-J., Xiao, H., Cao, C.-X. *Anal. Chim. Acta* 2017, 982, 200–208.
- 330 [9] Dong, Y.-C., Shao, J., Yin, X.-Y., Fan, L., Cao, C.-X. *J. Sep. Sci.* 2011, 34, 1683–1691.
- 331 [10] Fakhfouri, A., Devendran, C., Collins, D. J., Ai, Y., Neild, A. 10.
- 332 [11] Lin, S., Zhi, X., Chen, D., Xia, F., Shen, Y., Niu, J., Huang, S., Song, J., Miao, J., Cui,
333 D., Ding, X. *Biosens. Bioelectron.* 2019, 129, 175–181.
- 334 [12] Zeming, K. K., Thakor, N. V., Zhang, Y., Chen, C.-H. *Lab. Chip* 2016, 16, 75–85.
- 335 [13] Lin, S., Yu, Z., Chen, D., Wang, Z., Miao, J., Li, Q., Zhang, D., Song, J., Cui, D. *Small*
336 2020, 16, 1903916.
- 337 [14] Lee, M.-L., Yao, D.-J. *Inventions* 2018, 3, 40.
- 338 [15] Zhang, J., Chintalaramulu, N., Vadivelu, R., An, H., Yuan, D., Jin, J., Ooi, C. H., Cock,
339 I. E., Li, W., Nguyen, N.-T. *Anal. Chem.* 2020, 92, 11558–11564.
- 340 [16] Rzhavskiy, A. S., Razavi Bazaz, S., Ding, L., Kapitannikova, A., Sayyadi, N., Campbell,
341 D., Walsh, B., Gillatt, D., Ebrahimi Warkiani, M., Zvyagin, A. V. *Cancers* 2019, 12, 81.
- 342 [17] Yamada, M., Nakashima, M., Seki, M. *Anal. Chem.* 2004, 76, 5465–5471.
- 343 [18] Lu, X., Xuan, X. *Anal. Chem.* 2015, 87, 4560–4565.
- 344 [19] Lu, X., Xuan, X. *Anal. Chem.* 2015, 87, 6389–6396.

- 345 [20] Ylbing, S. *Research on Laser Direct Writing System and its Lithography Properties*, p.
346 10.
- 347 [21] Liu, Z., Li, J., Yang, J., Song, Y., Pan, X., Li, D. *Microfluid. Nanofluidics* 2017, 21, 4.
- 348 [22] Hongbin, Y., Guangya, Z., Siong, C. F., Shouhua, W., Feiwen, L. *Sens. Actuators B*
349 *Chem.* 2009, 137, 754–761.
- 350 [23] Nieuwstadt, H. A., Seda, R., Li, D. S., Fowlkes, J. B., Bull, J. L. *Biomed. Microdevices*
351 2011, 13, 97–105.
- 352 [24] Di Carlo, D., Irimia, D., Tompkins, R. G., Toner, M. *Proc. Natl. Acad. Sci.* 2007, 104,
353 18892–18897.
- 354 [25] Nieuwstadt, H. A., Seda, R., Li, D. S., Fowlkes, J. B., Bull, J. L. *Biomed. Microdevices*
355 2011, 13, 97–105.
- 356 [26] Li, D., Shao, X., Bostwick, J. B., Xuan, X. *Microfluid. Nanofluidics* 2019, 23, 125.
- 357 [27] Squires, T. M., Quake, S. R. *Rev. Mod. Phys.* 2005, 77, 977–1026.
- 358 [28] Jelly, T. O., Busse, A. *Int. J. Heat Fluid Flow* 2019, 80, 108485.
- 359 [29] Yuan, D., Tan, S. H., Zhao, Q., Yan, S., Sluyter, R., Nguyen, N. T., Zhang, J., Li, W.
360 *RSC Adv.* 2017, 7, 3461–3469.
- 361 [30] Nam, J., Namgung, B., Lim, C. T., Bae, J.-E., Leo, H. L., Cho, K. S., Kim, S. J.
362 *Chromatogr. A* 2015, 1406, 244–250.
- 363 [31] Singh, J., Kumar, C. V. A. *Rheol. Acta* 2019, 58, 709–718.
- 364 [32] Liu, C., Hu, G., Jiang, X., Sun, J. *Lab. Chip* 2015, 15, 1168–1177.
- 365 [33] Lu, X., Liu, C., Hu, G., Xuan, X. *J. Colloid Interface Sci.* 2017, 500, 182–201.
- 366 [34] Fei, T., Qiang, F., Chen, Q., Liu, C., Li, T., Sun, J. *Microfluid. Nanofluidics* 2019, 9.